



⑫ **EUROPEAN PATENT APPLICATION**
published in accordance with Art.
158(3) EPC

⑳ Application number: **93919631.7**

⑤① Int. Cl.⁵: **A61M 29/00**

㉔ Date of filing: **08.09.93**

⑧⑥ International application number:
PCT/JP93/01277

⑧⑦ International publication number:
WO 94/05364 (17.03.94 94/07)

㉓ Priority: **08.09.92 JP 239849/92**

④③ Date of publication of application:
21.09.94 Bulletin 94/38

⑧④ Designated Contracting States:
CH DE FR GB IT LI SE

⑦① Applicant: **KABUSHIKIKAISHA IGAKI IRYO**
SEKEI
1-21, Wakakusa 2-chome
Kusatsu-shi, Shiga 525 (JP)

⑦② Inventor: **IGAKI, Keiji**
1-21, Wakakusa 2-chome
Kusatsu-shi, Shiga 525 (JP)

⑦④ Representative: **TER MEER - MÜLLER -**
STEINMEISTER & PARTNER
Mauerkircherstrasse 45
D-81679 München (DE)

⑤④ **VESSEL STENT AND VESSEL STENT INSERTION DEVICE.**

⑤⑦ This invention discloses a vessel stent which is inserted into a vessel such as a blood vessel and retains the shape of the vessel, and a vessel stent insertion device. The vessel stent consists of filaments of continuous in-vivo absorbable polymer fiber, and the filaments are so shaped as to extend in zigzag along the peripheral surface of a cylindrical member, a tubular member, etc. Examples of the in-vivo absorbable polymer are polylactic acid, poly-

glycolic acid, polyglactin, polydioxanone, polyglyconate, and copolymers between the polyglycolic acid or polylactic acid and ϵ -caprolactone. The vessel stent insertion device puts the vessel stent over a balloon formation portion near the distal end of a catheter and bonds it by a biocompatible material such as the biodegradable polymer (e.g. polylactic acid), water-soluble protein, fibrin paste.

EP 0 615 769 A1

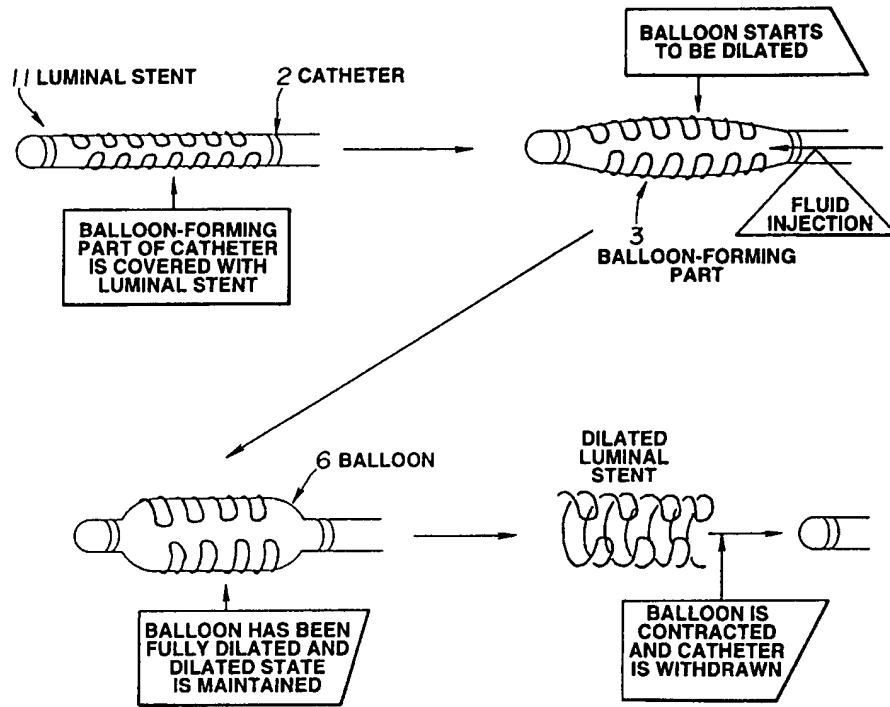


FIG.5

TECHNICAL FIELD

This invention relates to a luminal stent adapted to be inserted into the vessel, such as a blood vessel, lymph vessel, bile duct vessel, ureter vessel or esophagus for maintaining the shape of the vessel. More particularly, it relates to a luminal stent inserting device for inserting the luminal stent to a desired site in the vessel.

BACKGROUND ART

As this type of the luminal stent, there is known a textile structure in which linear longitudinal and transversal materials of stainless steel or the like are woven or knitted in a tube, and which may be enlarged and fitted to a site of an vasculogenetic operation.

However, this known type of the luminal stent suffers from the problem that it is harder and likely to apply the stress to the vessel to produce inflammation or excess hypertrophy susceptible to re-constriction in the vessel, and that the stent is left semi-permanently as a foreign matter in the living body which by nature acts to dispel such foreign matter.

If the luminal stent, such as a metal stent, which is left in the vessel semi-permanently or for a period longer than is necessary, is inserted into the vessel, it tends to act as a kind of a nucleus around which re-constriction is likely to occur in the vessel. In addition, if a part of the vessel in the vicinity of the stent is injured, there is a risk that the cells on the inner wall of the vessel increase in number due to multiplication to reduce the inner diameter of the vessel.

DISCLOSURE OF THE INVENTION

It is an object of the present invention to provide a luminal stent which is less susceptible to re-constriction in the vessel or reduction in the inner vessel diameter, and a device for inserting the luminal stent.

That is, the present invention is characterized in that a yarn formed of a continuous bioabsorbable polymer fibers is formed in a non-woven non-knitted state in a shape conforming to the peripheral surface of an imaginary tubular member, and in that such luminal stent is fitted on a balloon-forming portion in the vicinity of the distal end of a catheter and bonded to the balloon-forming portion by means of a bio-compatible material which does not cause any rejection symptoms.

The present invention includes a tubular luminal stent prepared in such a manner that the yarn formed of a continuous bioabsorbable polymer fibers is formed in a non-woven non-knitted

state in a shape conforming to the peripheral surface of an imaginary tubular member. The stent prepared in this manner is superior in pliability and shape retentivity to other cloths, that is, non-woven fabrics like felt or a customary woven cloth prepared from weft and warp yarns. The knitted luminal stent may be further improved in pliability and shape retentivity by heat treatment (heat-setting).

The above-mentioned luminal stent is inserted into the site of vasculogenesis via a catheter provided with a balloon. If, after the luminal stent is fitted on the balloon-forming portion, the solution of the bioabsorbable polymer is applied for bonding the luminal stent to the balloon-forming portion, the luminal stent may be prevented from being deviated in its position at the time of insertion of the catheter into the vessel.

With the above-described luminal stent of the present invention, the inflammation or excess hypertrophy of the vessel is not produced and hence re-constriction may be prevented from occurring. Also, the luminal stent disappears in several months by being absorbed into the living tissue and is therefore convenient for the living body.

In addition, with the device for inserting and fixing the luminal stent of the present invention, since the luminal stent is immobilized in the balloon-forming portion, the luminal stent may be reliably inserted and fixed in the vessel.

BRIEF DESCRIPTION OF THE DRAWINGS

Fig.1 is a schematic view showing several morphological examples of bioabsorbable polymer fibers in the non-woven non-knitted state.

Fig.2 is a schematic side view showing an example of a luminal stent to which the present invention is applied.

Fig.3 is a schematic side view showing another example of a luminal stent to which the present invention is applied.

Fig.4 illustrates the process of producing a luminal stent.

Fig.5 illustrates the process of inserting and placing the luminal stent in place within the vessel.

Fig.6 illustrates an alternative method for reducing the diameter of a luminal stent knitted with the yarn formed of PGA fibers.

Fig.7 shows another example of a device for inserting a luminal stent formed of knitted goods.

Fig.8 schematically illustrates a vessel and the state of insertion of the luminal stent, where A shows the morphology of an exemplary vessel, B shows the state of insertion of the luminal stent, and C shows, as a comparative example, the state of poor insertion of a conventional luminal stent.

Fig.9 illustrates that the luminal stent can be inserted into and placed at various sites within the vessel.

BEST MODE FOR CARRYING OUT THE INVENTION

The present invention is concerned with a luminal stent comprising a tubular body of the yarn of the bioabsorbable polymer fibers, and a luminal stent inserting device in which the stent is applied over a balloon-forming portion of a catheter.

The bioabsorbable polymers include polylactic acid (PLA), polyglycol acid (PGA), polyglactin (polyglycol acid - polylactic acid copolymer), polydioxanone, polyglyconate (trimethylene carbonate - glycolide copolymer), and a copolymer of ϵ - caprolactone with polyglycol acid or polylactic acid.

A variety of materials, including pharmaceuticals, may be mixed into the bioabsorbable polymer. These materials may also be affixed to the fiber surface.

The luminal stent of the present invention is inserted into the site of vasculogenesis via a catheter fitted with a balloon and is mounted in place by being extended as a result of inflation of the balloon. Although the shape of the luminal stent thus inserted is maintained for several weeks to several months after the insertion, it is formed of the bioabsorbable polymer fibers and hence disappears by being absorbed into the living tissue after the lapse of several months after the insertion.

In addition, if a material impermeable to X-rays is mixed into the bioabsorbable polymer, the state of the luminal stent may be recognized on irradiation of X-rays from outside after its insertion.

The luminal stent of the present invention essentially consists of a single yarn entwined around the peripheral surface of a tubular member into a tubular form without weaving or knitting the yarn. Although the yarn is entwined around the peripheral surface of the tubular member, it is not in the wound or coiled state around the tubular member. That is, the yarn of the bioabsorbable polymer fibers is meandered or coiled into one or more loops, as shown in Figs.1a to 1g, for forming a planar yarn mass formed by meandered and/or coiled bioabsorbable polymer fibers, which yarn mass is entwined around the tubular member for producing a fiber mass extending along a curved surface.

Fig.2 shows an example of a luminal stent according to the present invention in which a meandering yarn formed of bioabsorbable polymer fibers is shaped into a tube. Fig.3 shows another example of a luminal stent according to the present invention in which a looped yarn formed of bioabsorbable polymer fibers is similarly shaped into a

tube.

When transporting the luminal stent of the present invention to a target site, it can be passed through various meandering vessels substantially more easily than the metal stent or the woven or knitted textile stent. That is, the luminal stent prepared from the yarn formed of bioabsorbable polymer fibers is able to follow any meandering path with excellent trackability, while it can be inserted as far as and fixed at a bent site because the yarn formed into a tubular shape by meandering without being woven or knitted exhibits strong extendibility and is not likely to injure the cavity. According to the present invention, in order for the luminal stent in the shape of a tube about 5 mm in diameter to be introduced into a vessel of the living body which is lesser in diameter, the tube is heat-set by heat treatment and thereby shrunk to a diameter of approximately 2 mm or less. The process is illustrated in Fig.4.

The heat-set luminal stent is inserted into the vessel in the manner shown in Fig.5, as will be explained subsequently,

Fig.6 shows another method of contracting the diameter of a luminal stent formed by shaping the yarn of PGA (polyglycol acid) polymer fibers. The method shown in Fig.6 has an advantage in that, since a tube formed of a heat-resistant resin or metal is not employed, the stent may be directly introduced into and fixed at a balloon forming area in the vicinity of a foremost part of a catheter.

The tubular luminal stent prepared by shaping a yarn of bioabsorbable polymer fibers has a diameter of approximately 4 to 5 mm and is heat-set by being housed in or gradually introduced into a tube of a heat-resistant resin or metal having an inner diameter of 1 to 3 mm and preferably 2 mm for producing a luminal stent having a diameter of approximately 2 mm, as shown in Fig.4.

In addition, the tubular luminal stent may be heat-set while in the larger diameter. Alternatively, the tubular luminal stent may be reduced in diameter and heat-set for maintaining good shaping properties. The heat setting not only is effective for maintaining the shape of the luminal stent but is meaningful in minimizing the stress applied to the inner wall of the vessel of the living body.

Meanwhile, by forming the bioabsorbable polymer fibers of PLA and PGA, and changing their mixing ratio, the time period required for the strength of the luminal stent of the present invention to be decreased to one-half of the original strength, or the time period until extinction of the luminal stent through absorption into the living body, may be freely controlled within a range from three weeks to three months.

If an agent impermeable to X-rays is mixed into the fibers at the time of spinning the fibers into

a yarn, the state of insertion of the luminal stent can be observed by the X-rays. Thrombolytic agents or anti-thrombotic agents, such as heparin, urokinase or t-PA, may also be mixed for optimum effects.

Furthermore, since the luminal stent of the present invention is formed of the yarn of bioabsorbable polymer fibers, and hence it disappears from the site of vasculogenesis in a preset period, carcinostatic agents or various other pharmaceutical may be mixed into or affixed on the fibers for concentrated administration of the pharmaceutical to the site of lesion.

In addition, the fibers making up the luminal stent of the present invention may be variegated in the cross-sectional shape thereof more easily than in the case of preparing the luminal stent of metal. That is, by setting the cross-sectional shape of the filaments on spinning so as to be of a hollow or profiled shape, such as an elliptical or a flower petal shape, or by employing monofilaments or multifilaments, it becomes possible to control biocompatibility or shape retention characteristics.

The yarn formed of a synthetic high molecular material may have its fiber surface processed in desired manner. With the yarn having the usual substantially circular cross-section and having its surface not processed in any particular manner, the yarn having the so-called profiled cross-section, or the yarn processed as described above, it becomes possible to deposit an anti-thrombotic material or a thrombolytic agent on the yarn or cells of the living body to promote multiplication of the endothelial cells of the living body or to a material impermeable to X-rays. In this case, longitudinally extending flutes or a variety of recesses may be formed on the yarn surface for improving the deposition efficiency.

If it is desired to increase the diameter of a constricted portion of the vessel to a diameter of, for example, 4 mm and to maintain this diameter, it is not increased at a time. That is, for avoiding the sudden stress being applied to the vessel and to the living body, the vessel is expanded initially to a diameter of 3 mm, using an expander having a balloon-forming portion having a diameter of approximately 0.8 to 1.2 mm, after which the catheter provided with a balloon is extracted. A catheter provided with a balloon, which catheter is not fitted with a luminal stent and is capable of only forming a balloon, is again inserted for enlarging the vessel to a diameter slightly larger than 4 mm. Subsequently, a knitted luminal stent is introduced and fixed at the balloon forming portion using a device for inserting and fixing the luminal stent of the present invention.

It is unnecessary to expand and form the vessel stepwise. Thus, it is possible to expand the

constricted portion of the vessel at a time to a desired diameter and subsequently proceed to the fitting of the luminal stent.

On the other hand, the luminal stent fitting device itself, consisting in a catheter fitted with a balloon and a luminal stent of the present invention fitted thereon, may be used for inserting and fixing the luminal stent in the vessel of the living body simultaneously with expansion of the vessel.

The device for inserting and fixing the luminal stent of the present invention in a constricted portion of the vessel of the living body is explained in detail. There is an area 3 in the vicinity of the distal end of a catheter 2 in which a balloon of a desired diameter may be formed by the liquid or the gas, such as an X-ray contrast medium, which is injected from a hollow portion in the catheter at a liquid pressure of 8 to 10 atmospheres, as shown in Fig.5. It is over this balloon-forming area 3, which is about 20 mm long, that a luminal stent 11 about 2 mm in diameter, as heat-set, is applied.

It is noted that the length of the balloon-forming area 3 or the diameter of the luminal stent 11 may be optionally set depending on the type of the vessel to be treated or the specific properties of the vessel.

Meanwhile, a guide wire acting as a leading wire when inserting the catheter into the vessel of a living body is occasionally mounted on the distal end of the catheter.

As for the insertion of the luminal stent, a mid part along the length of the balloon-forming area of the catheter is formed with a communication orifice via which the fluid injected for balloon formation is caused to flow out at the mid portion of the catheter so as to be charged into a space between it and a thin film forming the balloon. It is via this orifice that the balloon is formed under a fluid pressure of 8 to 10 atmospheres, with the ballooned state being kept for 30 to 60 seconds and occasionally for a longer time duration. At this time, the balloon undergoes a kind of plastic deformation and is maintained under the inflated condition under the inflating pressure exerted by the balloon. The inflated shape is maintained by changes in the polymer itself on the molecular level or the yarn shaped into a tube is expanded in the radial direction for maintaining the expanded shape.

Fig.5 shows the process of inserting and fitting the luminal stent of the present invention in the vessel of a living body. As shown therein, the balloon is inflated and subsequently contracted to permit the catheter 2 in its entirety to be withdrawn from the luminal stent.

Fig.7 shows another embodiment of a luminal stent inserting and fitting device according to the present invention. A catheter fitted with a balloon, on which the luminal stent 11 is subsequently

wrapped, is encased within a sheath 5. The resulting assembly is inserted into the vessel of the living body. The sheath is extracted slightly and the balloon is inflated and maintained in the inflated state. The balloon is contracted and the sheath 5 is extracted along with the catheter 2 so that the luminal stent is left in the vessel of the living body.

Meanwhile, the film for balloon formation may be formed of any of a variety of synthetic high molecular material, such as polyethylene terephthalate or polyethylene.

It is noted that the luminal stent of the present invention may be inserted and fitted in a bend of the vessel to conform to its shape, as shown in Fig.8. The state of the stent as inserted and fitted is shown in Fig.8B. A metal stent formed of a woven or knitted textile of linear longitudinal and transverse materials and subsequently formed into a tubular form is shown in Fig.8C in the state of being inserted into and fitted in a bend of the vessel. Such stent is flexed in the bend of the vessel so that the normal shape of the vessel cannot be maintained at the site. Conversely, the luminal stent of the present invention is able to follow a branched section in the vessel with good trackability so that it can reach any constricted site in the vessel, as discussed previously.

In Fig.8A, showing a typical shape of the vessel of a living body, the site shown by an arrow a represents a site assumed to be the mounting site for the luminal stent of the present invention.

The luminal stent of the present invention, as formed by the yarn of the bioabsorbable polymer fibers and heat-set, may be adapted to a vessel of an arbitrary thickness by means of the luminal stent inserting and fixing device according to the present invention. If it is assumed that the luminal stent is applied to a site where the vessel is enlarged to a diameter of approximately 4 mm or larger on inflation of the balloon, the luminal stent may be applied to the vessel site having the diameter of 2.5 mm by controlling the degree of inflation of the balloon. The luminal stent may similarly be applied to a vessel site having the diameter of 3 to 4 mm. That is, the luminal stent may be applied to any site shown in Fig.9 using the same catheter provided with the balloon. The reason is that the inner diameter of the luminal stent may be maintained at a diameter corresponding to the diameter of the inflated balloon.

If vessel re-constriction is produced in several months after the luminal stent of the present invention is decomposed and absorbed to the living body, the luminal stent may be applied again to the same site because the stent is formed of biodegradable and absorbable polymer material.

The luminal stent of the present invention, as described above, is not susceptible to inflammation

or excess hypertrophy of the vessel, and hence the re-constriction may be prevented from occurrence. In addition, the luminal stent is compatible with the living body because it is vanished in several months by being absorbed by the living tissue.

If an agent impermeable to X-rays is applied to the bioabsorbable polymer fibers or the yarn, the state of insertion of the luminal stent may be checked easily by irradiation of X-rays from outside.

Also, the luminal stent may be applied on the balloon-forming portion of the catheter provided with the balloon according to the present invention for inserting and fitting the stent at any desired location in the vessel.

Meanwhile, if the luminal stent of the present invention is applied over the balloon-forming portion of the catheter fitted with the balloon for fixing the stent at a desired site in the vessel, it may occur that the fixing position of the luminal stent is deviated due to contact of the stent with the inner wall of the vessel. If the luminal stent is deviated in its position and disengaged from the balloon forming region, it becomes difficult to realize an optimum expanded position.

Thus it is desirable to apply a bio-compatible material on the luminal stent applied over the balloon-forming region by way of "sizing" for immobilizing the luminal stent at the balloon forming region. The material that may be employed as an adhesive or sizing agent is a bio-compatible material enumerated by an in vivo decomposable polymer, such as polylactic acid (PLA), water-soluble protein, such as gelatin, or fibrin sizing agent.

If, for example, PLA is dissolved as a solute in a solvent to give a solution which is coated on the stent and dried, the solution is left as a solid film to play the role of an adhesive. However, this method cannot be applied to the PLA stent because the PLA stent is dissolved in the solution. Thus it is necessary to employ some other bio-compatible material for the PLA stent.

Meanwhile, the bio-compatible material, used as the adhesive, may be applied to the stent in its entirety, or only to the overlapped region of the bioabsorbable polymer fibers.

Experiment 1

A yarn of polylactic acid fibers, admixed with barium sulfate, was meandered and applied to the peripheral surface of a tubular-shaped member to form a luminal stent. A plurality of such luminal stents, each being 4 mm in diameter and 20 mm in length, were applied to the coronary artery of a test animal, using a catheter fitted with a balloon. Observation by X-ray radiation revealed that the shape of the stent was maintained substantially un-

changed for about 3 to 6 months and disappeared in about 6 to 12 months by being absorbed by the living tissue. During this period, inflammation or excess hypertrophy of the endothelial cells of the blood vessel was not observed.

Experiment 2

A yarn of polyglycol acid fibers, admixed with barium sulfate, was looped to be a plane-shaped and applied to the peripheral surface of a tubular-shaped member to form a luminal stent. A plurality of such luminal stents, each being 4 mm in diameter and 20 mm in length, were applied to the femoral artery of a test animal. Observation by X-ray radiation revealed that the shape of the stent was maintained substantially unchanged for about 2 to 6 weeks and absorbed by the living body in about 2 to 3 months. During this period, inflammation or excess hypertrophy of the endothelial cells of the blood vessel was not observed.

Claims

1. A luminal stent in which a yarn of continuous bioabsorbable polymer fibers is formed in a non-woven non-knitted state in a shape conforming to peripheral surface of an imaginary tubular member.
2. A luminal stent in which a yarn of continuous bioabsorbable polymer fibers is formed in a meandering state in a shape conforming to peripheral surface of an imaginary tubular member.
3. The luminal stent as claimed in claim 1 or 2, characterized in that the bioabsorbable polymer is at least one selected from the group consisting of polylactic acid, polyglycol acid, polyglactin (polyglycol acid -polylactic acid copolymer), polydioxanone, polyglyconate (trimethylene carbonate - glycolide copolymer), and a copolymer of ϵ -caprolactone with polyglycol acid or polylactic acid.
4. The luminal stent as claimed in claim 1 or 2, characterized in that the bioabsorbable polymer fibers are circular, non-circular or hollow in cross-section.
5. The luminal stent as claimed in claim 1 or 2, characterized in that the bioabsorbable polymer fibers present surface irregularities.
6. The luminal stent as claimed in claim 1 or 2, characterized in that at least one of an agent impermeable to X-rays, a carcinostatic agent

and an anti-thrombotic agent is mixed into the bioabsorbable polymer fibers.

7. The luminal stent as claimed in claim 1 or 2, characterized in that at least one of an agent impermeable to X-rays, a carcinostatic agent, an anti-thrombotic agent and cells of a living body is deposited on the surface of the bioabsorbable polymer fibers.
8. A method for producing a luminal stent comprising guiding a planar mass formed of a yarn of bioabsorbable polymer fibers along peripheral surface of a tubular member for shaping said planar mass substantially into a tubular member presenting a curved surface.
9. The method for producing the luminal stent as claimed in claim 8, further comprising heat-setting the tubular member having the curved surface for reducing the diameter of the tubular member as compared to the diameter during shaping.
10. A device for applying a luminal stent comprising a catheter having a balloon-forming portion at a distal end thereof and the luminal stent as claimed in claim 1 or 2, said luminal stent being fitted over said balloon-forming portion.
11. The device for applying a luminal stent as claimed in claim 10, wherein the luminal stent is coated with a bio-compatible material and thereby affixed to the balloon-forming portion.
12. The device for applying a luminal stent as claimed in claim 11, characterized in that the bio-compatible material is at least one selected from an *in vivo* decomposable polymer, a water-soluble polymer, water-soluble protein and fibrin sizing agent.
13. The device for applying a luminal stent as claimed in claim 11, characterized in that the bio-compatible material is polylactic acid (PLA).

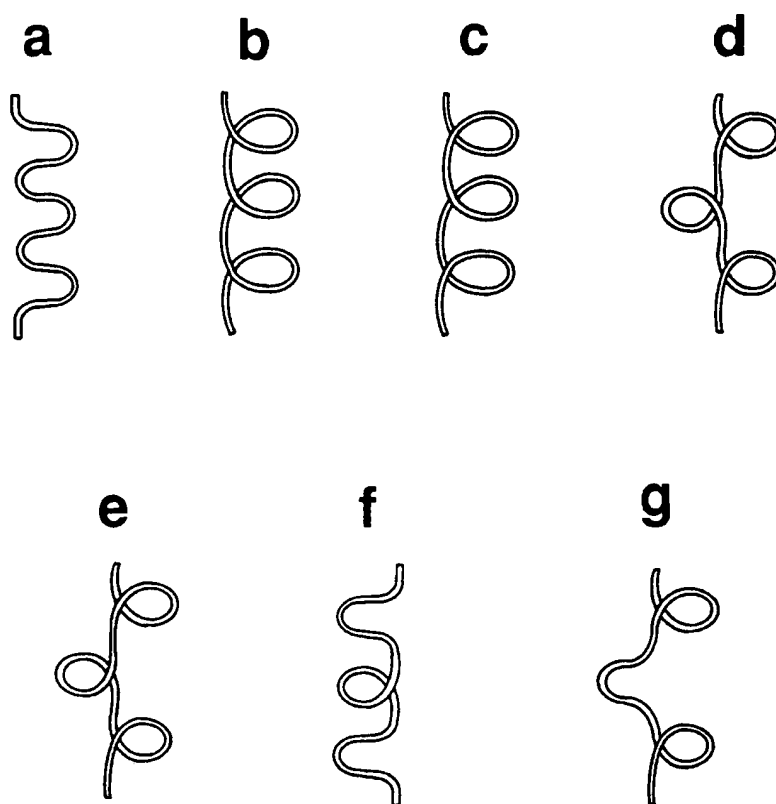


FIG.1

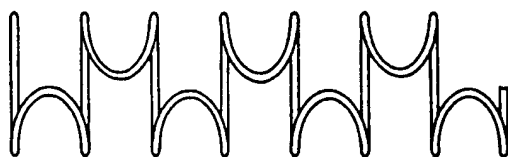


FIG.2

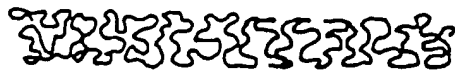


FIG.3

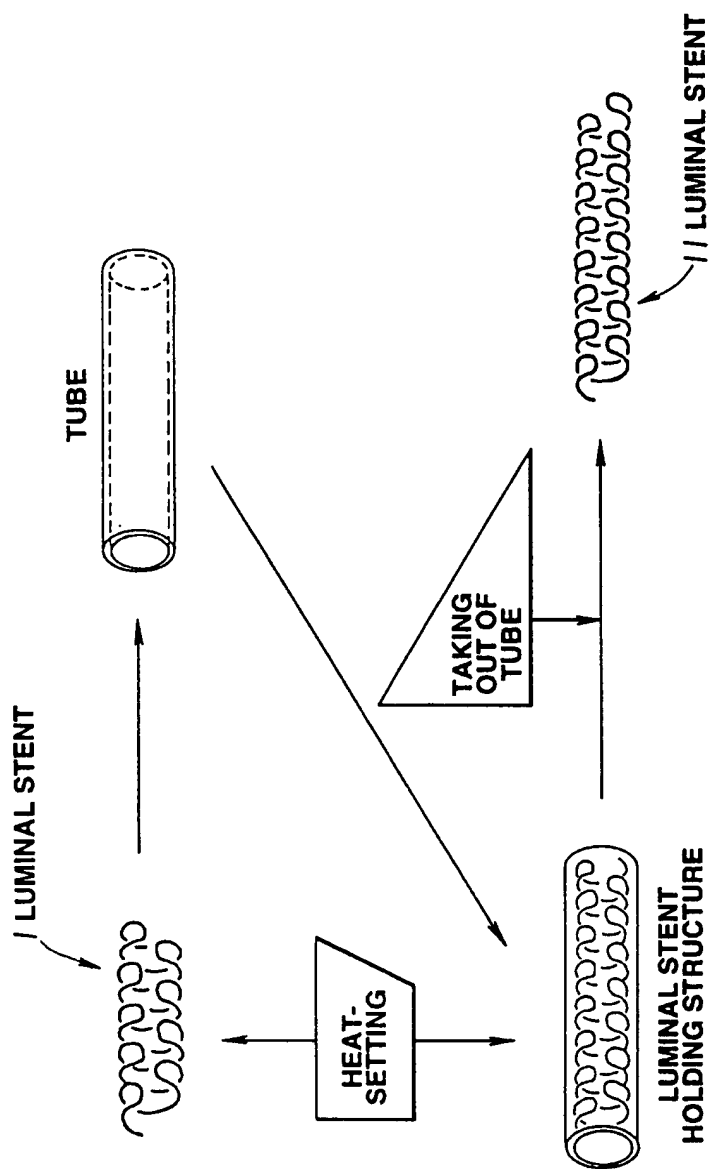


FIG.4

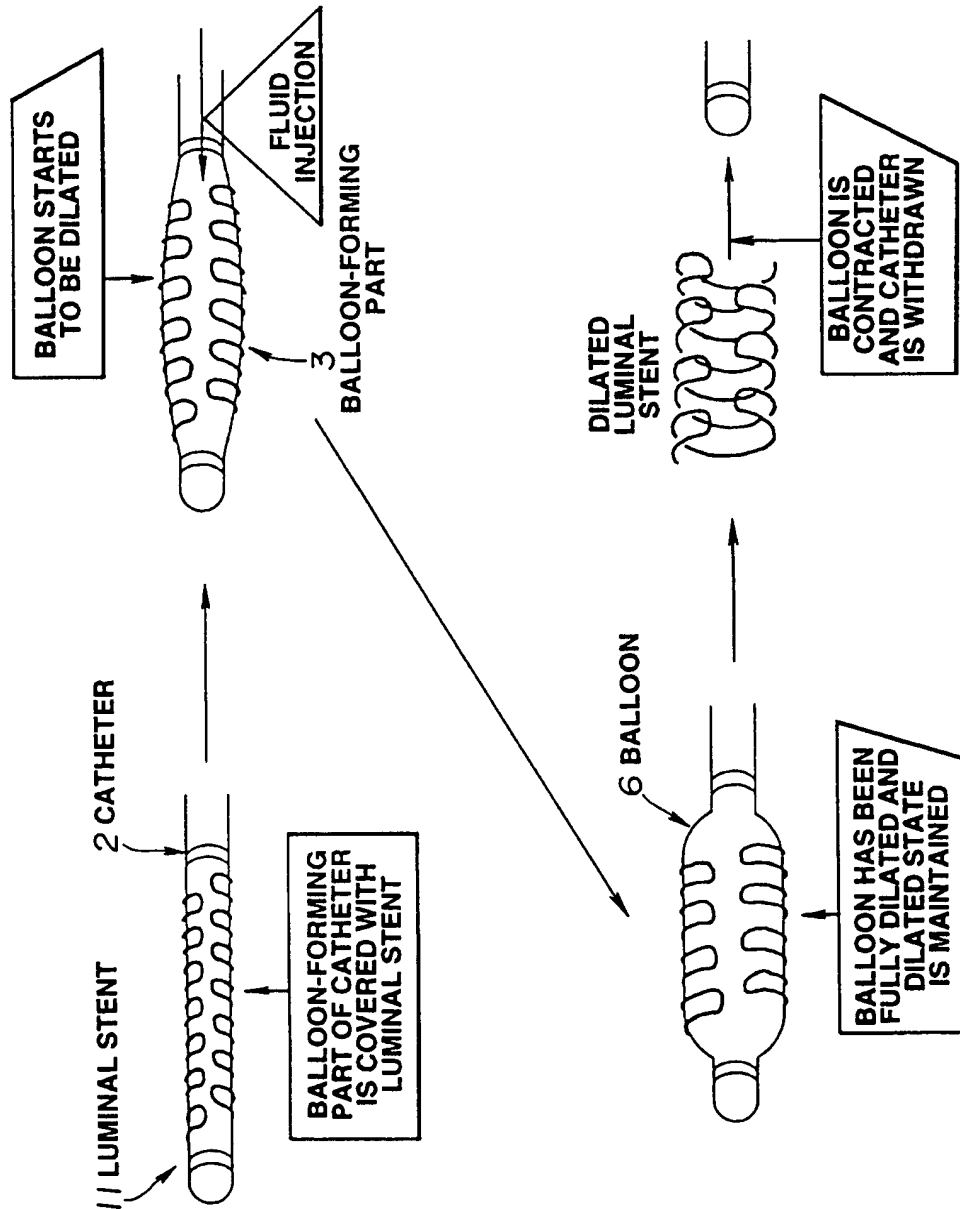


FIG.5

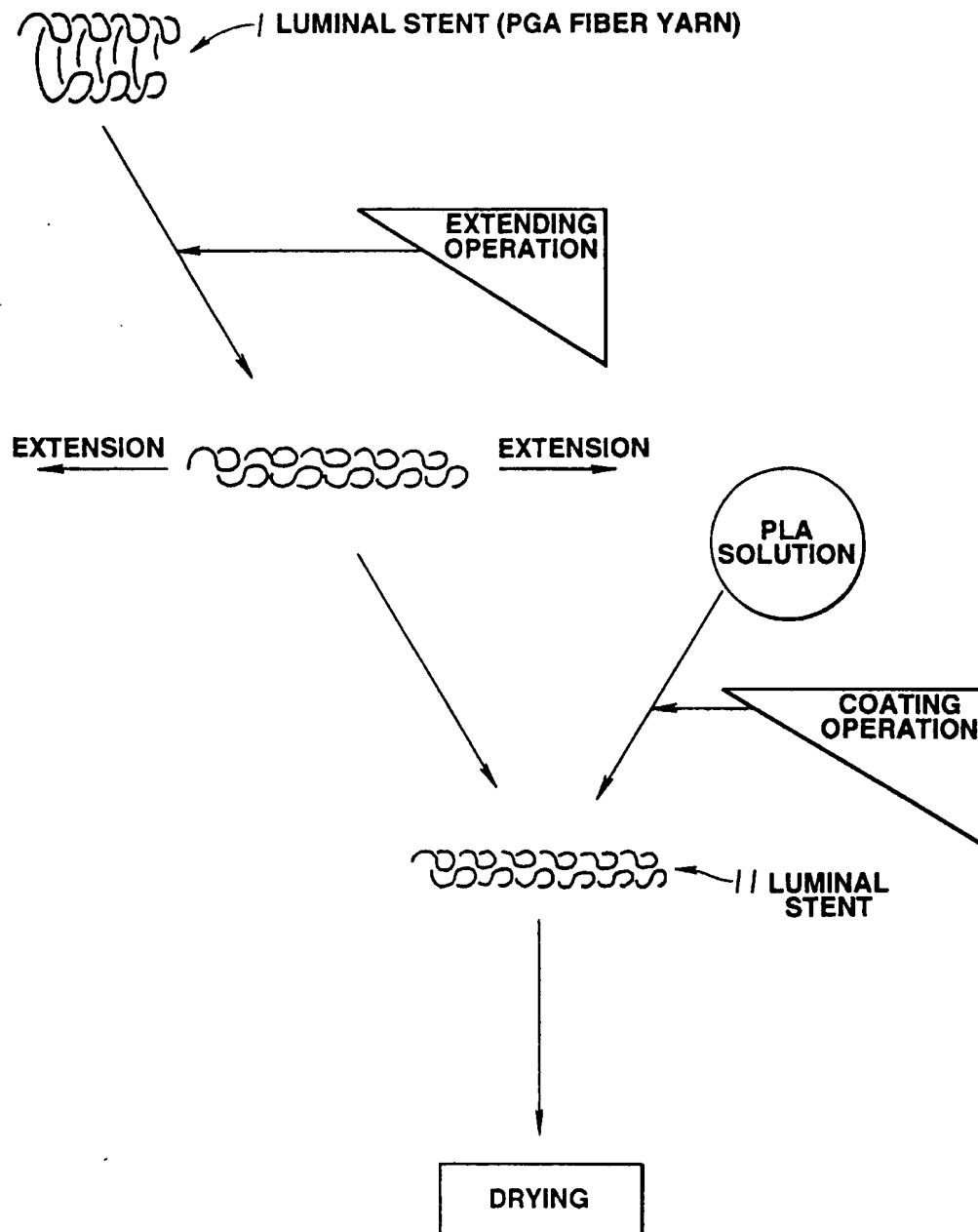


FIG.6

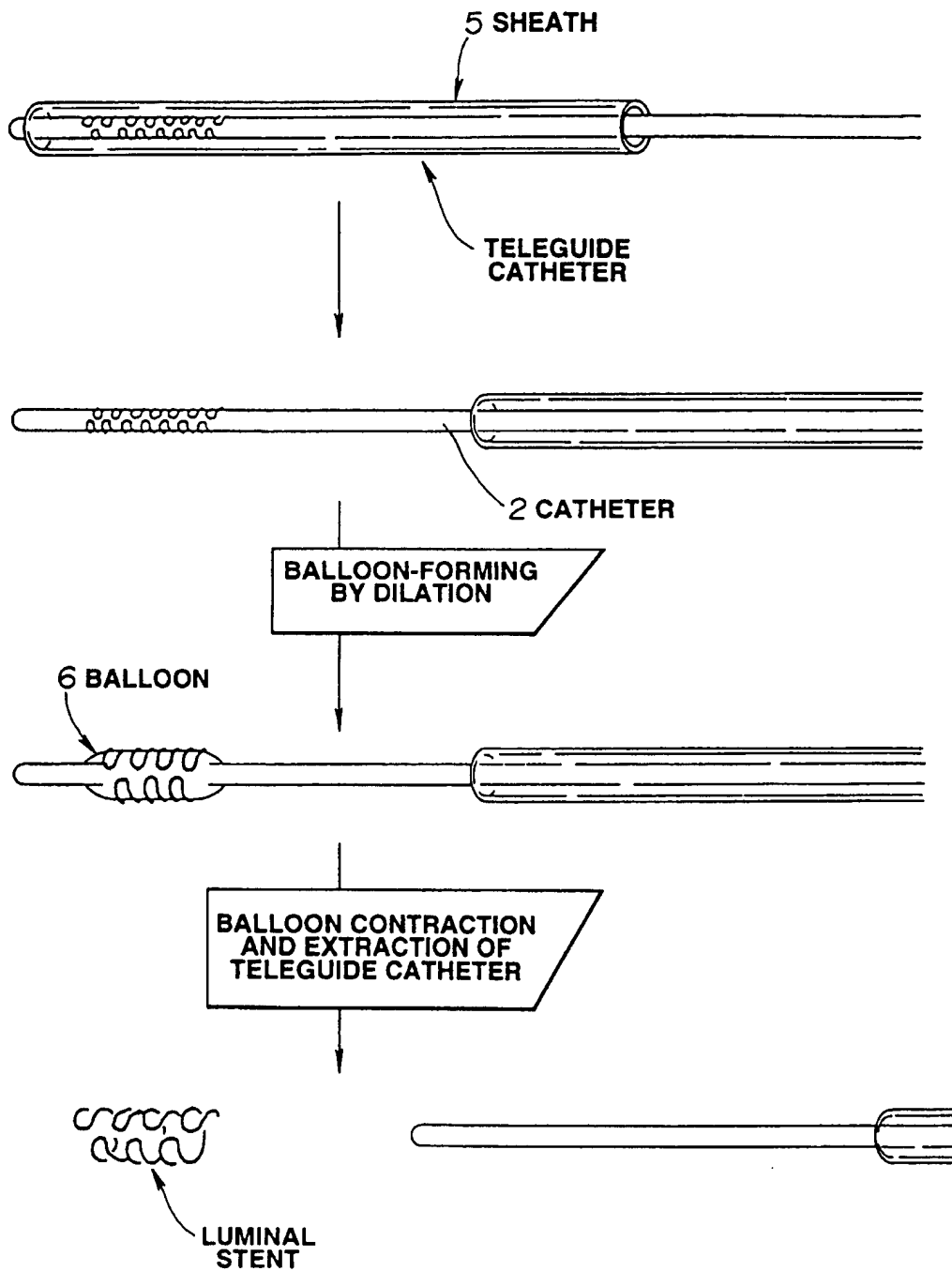


FIG.7

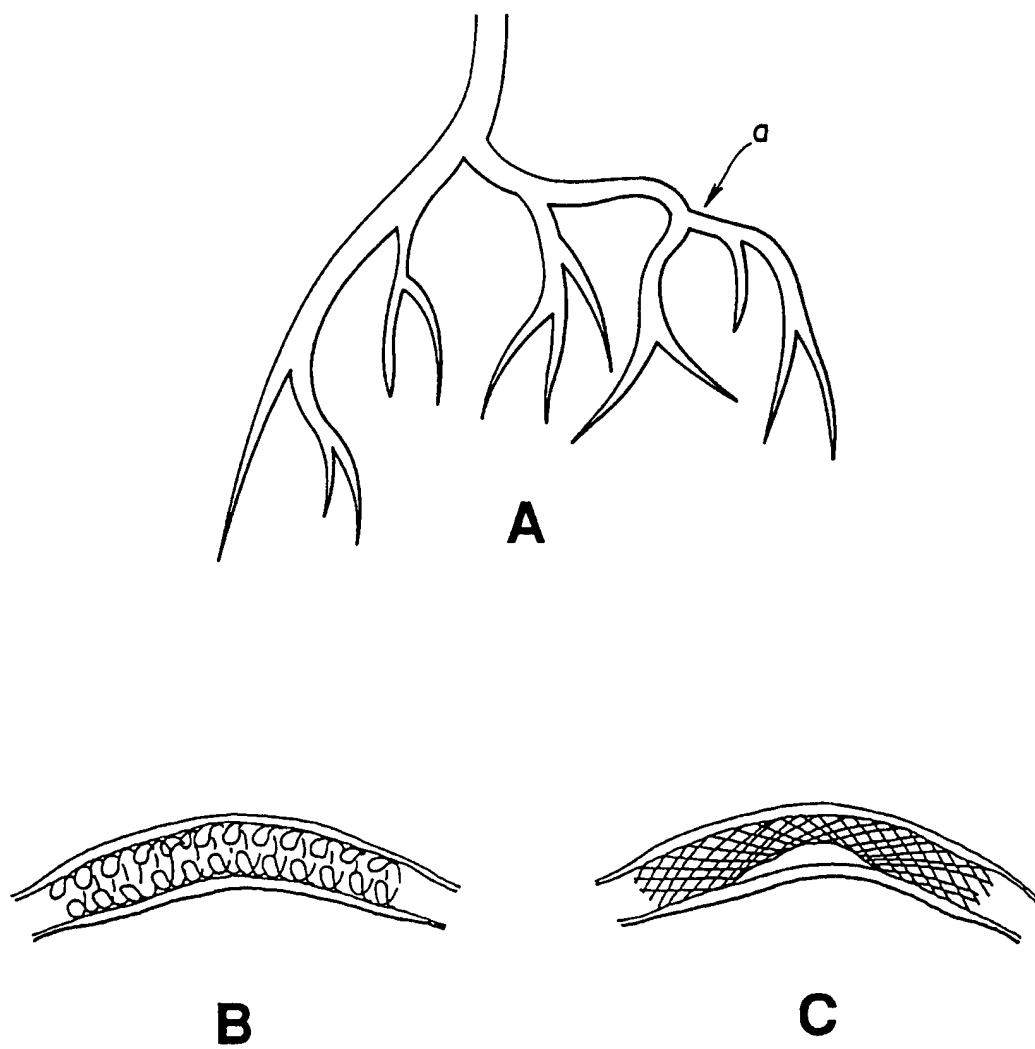


FIG.8

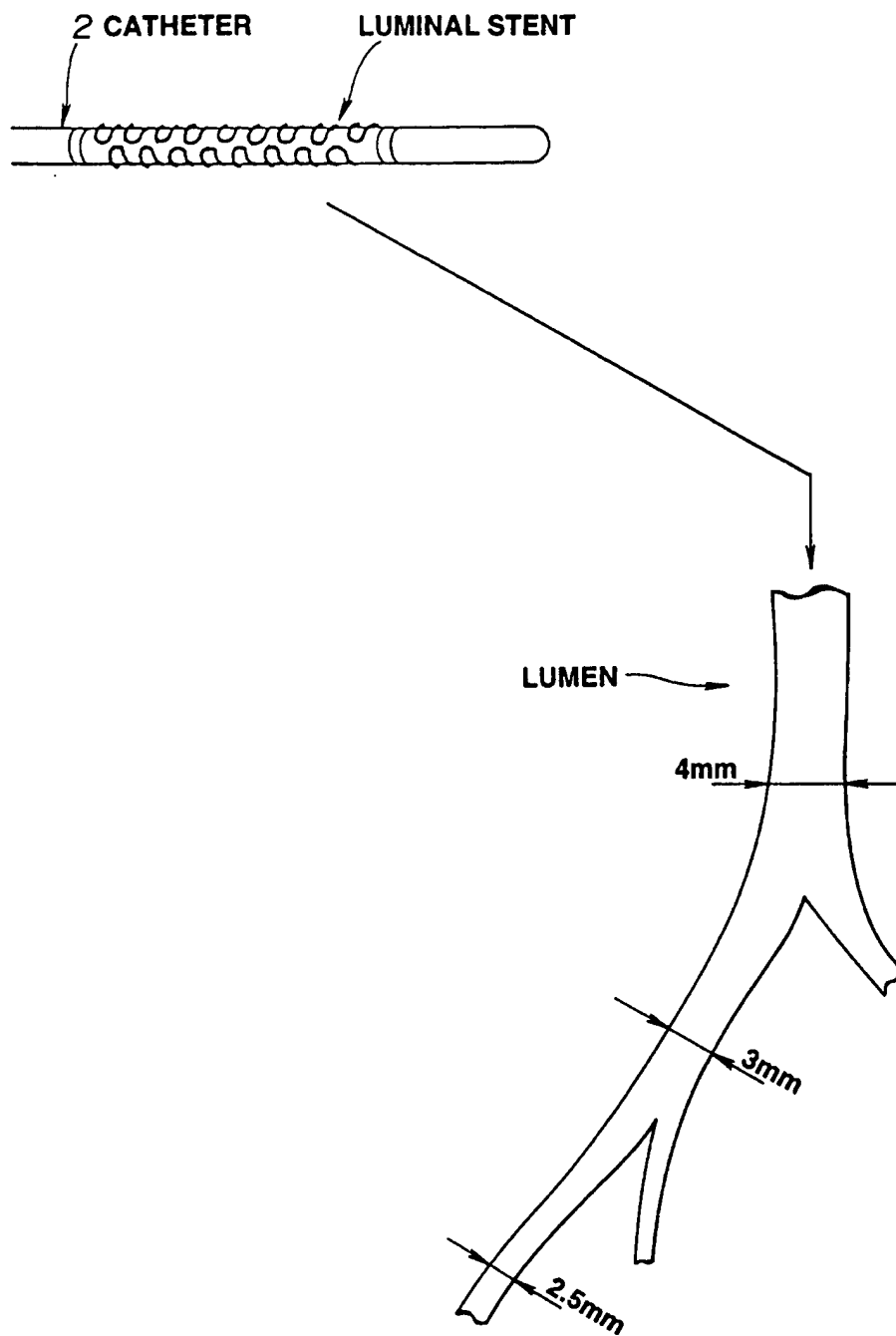


FIG.9

INTERNATIONAL SEARCH REPORT

International application No.

PCT/JP93/01277

A. CLASSIFICATION OF SUBJECT MATTER Int. Cl ⁵ A61M29/00 According to International Patent Classification (IPC) or to both national classification and IPC		
B. FIELDS SEARCHED Minimum documentation searched (classification system followed by classification symbols) Int. Cl ⁵ A61M29/00-29/02 Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched Jitsuyo Shinan Koho 1926 - 1993 Kokai Jitsuyo Shinan Koho 1971 - 1993 Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)		
C. DOCUMENTS CONSIDERED TO BE RELEVANT		
Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
Y	JP, A, 3-205059 (Bristol-Myers Squib Co.), September 6, 1991 (06. 09. 91), Full descriptions & EP, A, 420541 & US, A, 5085629	1-3
Y	US, A, 5100429 (BARD. C. R. Inc.), March 31, 1992 (31. 03. 92), Full descriptions (Family: none)	1-3
P	JP, A, 5-103830 (Gunze Ltd.), April 27, 1993 (27. 04. 93), Full descriptions (Family: none)	1-3
<input checked="" type="checkbox"/> Further documents are listed in the continuation of Box C. <input type="checkbox"/> See patent family annex.		
* Special categories of cited documents: "A" document defining the general state of the art which is not considered to be of particular relevance "E" earlier document but published on or after the international filing date "L" document which may throw doubts on priority claim(s) or which is cited to establish the publication date of another citation or other special reason (as specified) "O" document referring to an oral disclosure, use, exhibition or other means "P" document published prior to the international filing date but later than the priority date claimed "T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention "X" document of particular relevance: the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone "Y" document of particular relevance: the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art "&" document member of the same patent family		
Date of the actual completion of the international search November 29, 1993 (29. 11. 93)		Date of mailing of the international search report December 21, 1993 (21. 12. 93)
Name and mailing address of the ISA/ Japanese Patent Office Facsimile No.		Authorized officer Telephone No.

(19)



Europäisches Patentamt
European Patent Office
Office européen des brevets



(11)

EP 0 615 769 B1

(12)

EUROPEAN PATENT SPECIFICATION

(45) Date of publication and mention
of the grant of the patent:

29.05.2002 Bulletin 2002/22

(51) Int Cl.7: **A61M 29/00**

(86) International application number:
PCT/JP93/01277

(21) Application number: **93919631.7**

(87) International publication number:
WO 94/05364 (17.03.1994 Gazette 1994/07)

(22) Date of filing: **08.09.1993**

(54) **VESSEL STENT AND VESSEL STENT INSERTION DEVICE**

GEFÄSSSTENT UND ZUGEHÖRIGE EINFÜHRUNGSVORRICHTUNG

EXTENSEUR DE VAISSEAU ET DISPOSITIF D'INSERTION

(84) Designated Contracting States:
CH DE FR GB IT LI SE

(30) Priority: **08.09.1992 JP 23984992**

(43) Date of publication of application:
21.09.1994 Bulletin 1994/38

(73) Proprietor: **KABUSHIKIKAISHA IGAKI IRYO
SEKKEI
Kyoto-shi, Kyoto 607-8035 (JP)**

(72) Inventor: **IGAKI, Keiji
Kusatsu-shi, Shiga 525 (JP)**

(74) Representative: **Müller, Frithjof E., Dipl.-Ing.
Müller Hoffmann & Partner
Patentanwälte
Innere Wiener Strasse 17
81667 München (DE)**

(56) References cited:

EP-A- 0 282 175	EP-A- 0 357 003
EP-A- 0 441 516	WO-A-90/01969
WO-A-91/17789	WO-A-93/06792
WO-A-93/15787	JP-A- 3 205 059
JP-A- 5 103 830	US-A- 5 100 429

Note: Within nine months from the publication of the mention of the grant of the European patent, any person may give notice to the European Patent Office of opposition to the European patent granted. Notice of opposition shall be filed in a written reasoned statement. It shall not be deemed to have been filed until the opposition fee has been paid. (Art. 99(1) European Patent Convention).

EP 0 615 769 B1

Description

TECHNICAL FIELD

[0001] This invention relates to a luminal stent adapted to be inserted into the vessel, such as a blood vessel, lymph vessel, bile duct vessel, ureter vessel or esophagus for maintaining the shape of the vessel. More particularly, it relates to a luminal stent inserting device for inserting the luminal stent to a desired site in the vessel.

BACKGROUND ART

[0002] As this type of the luminal stent, there is known a textile structure in which linear longitudinal and transversal materials of stainless steel or the like are woven or knitted in a tube, and which may be enlarged and fitted to a site of an vasculogenetic operation.

[0003] However, this known type of the luminal stent suffers from the problem that it is harder and likely to apply the stress to the vessel to produce inflammation or excess hypertrophy susceptible to re-constriction in the vessel, and that the stent is left semi-permanently as a foreign matter in the living body which by nature acts to dispel such foreign matter.

[0004] If the luminal stent, such as a metal stent, which is left in the vessel semi-permanently or for a period longer than is necessary, is inserted into the vessel, it tends to act as a kind of a nucleus around which re-constriction is likely to occur in the vessel. In addition, if a part of the vessel in the vicinity of the stent is injured, there is a risk that the cells on the inner wall of the vessel increase in number due to multiplication to reduce the inner diameter of the vessel.

[0005] In EP 0 282 175 A1 an expandable stent comprising a wire formed into a certain serpentine configuration formed into a cylindrical shape is disclosed. The wire is preferably made of a malleable material such as annealed stainless steel, tungsten or platinum. In WO 91/17789 a stent made of bioabsorbable material woven into a diamond-braided pattern is disclosed. Metal stents or woven textile stents, however, have the disadvantage that their trackability upon passage through meandering vessels is unsatisfactory.

[0006] Document EP-A-0 357 003 discloses a stent which is formed of a biodegradable and biocompatible polymer wire. This wire forms an undulating length of a generally sinusoidal character, that length being wound in a generally helical manner.

DISCLOSURE OF THE INVENTION

[0007] It is an object of the present invention to provide a luminal stent which is less susceptible to re-constriction in the vessel or reduction in the inner vessel diameter, a method for producing such luminal stent, and a combination for applying the luminal stent.

[0008] To solve this object, the present invention pro-

vides a luminal stent as described in claim 1, a method for producing the luminal stent as specified in claim 7 and a combination for applying the luminal stent as defined in claim 9. Preferred embodiments of the invention are described in the subclaims.

[0009] A yarn formed of continuous bioabsorbable polymer fibers is formed in a non-woven non-knitted state in a shape conforming to the peripheral surface of an imaginary tubular member, and such luminal stent is fitted on a balloon-forming portion in the vicinity of the distal end of a catheter and bonded to the balloon-forming portion by means of a biocompatible material which does not cause any rejection symptoms.

[0010] A tubular luminal stent is prepared in such a manner that the yarn formed of continuous bioabsorbable polymer fibers is formed in a non-woven non-knitted state in a shape conforming to the peripheral surface of an imaginary tubular member. The stent prepared in this manner is superior in pliability and shape retentivity to other cloths, that is, non-woven fabrics like felt or a customary woven cloth prepared from weft and warp yarns. The non-knitted stent may be further improved in pliability and shape retentivity by heat treatment (heat-setting).

[0011] The above-mentioned luminal stent is inserted into the site of vasculogenesis via a catheter provided with a balloon. If, after the luminal stent is fitted on the balloon-forming portion, the solution of the bioabsorbable polymer is applied for bonding the luminal stent to the balloon-forming portion, the luminal stent may be prevented from being deviated in its position at the time of insertion of the catheter into the vessel.

[0012] With the above-described luminal stent of the present invention, the inflammation or excess hypertrophy of the vessel is not produced and hence re-constriction may be prevented from occurring. Also, the luminal stent disappears in several months by being absorbed into the living tissue and is therefore convenient for the living body.

[0013] In addition, with the device for inserting and fixing the luminal stent of the present invention, since the luminal stent is immobilized in the balloon-forming portion, the luminal stent may be reliably inserted and fixed in the vessel.

BRIEF DESCRIPTION OF THE DRAWINGS

[0014] Fig. 1 is a schematic view showing several morphological examples of bioabsorbable polymer fibers in the non-woven non-knitted state.

[0015] Fig. 2 is a schematic side view showing an example of a luminal stent to which the present invention is applied.

[0016] Fig. 3 is a schematic side view showing another example of a luminal stent to which the present invention is applied.

[0017] Fig. 4 illustrates the process of producing a luminal stent.

[0018] Fig.5 illustrates the process of inserting and placing the luminal stent in place within in the vessel.

[0019] Fig.6 illustrates an alternative method for reducing the diameter of a luminal stent with the yarn formed of PGA fibers.

[0020] Fig.7 shows another example of a device for inserting a luminal stent formed of goods.

[0021] Fig.8 schematically illustrates a vessel and the state of insertion of the luminal stent, where A shows the morphology of an exemplary vessel, B shows the state of insertion of the luminal stent, and C shows, as a comparative example, the state of poor insertion of a conventional luminal stent.

[0022] Fig.9 illustrates that the luminal stent can be inserted into and placed at various sites within the vessel.

BEST MODE FOR CARRYING OUT THE INVENTION

[0023] The present invention is concerned with a luminal stent comprising a tubular body of the yarn of the bioabsorbable polymer fibers, and a luminal stent inserting device in which the stent is applied over a balloon-forming portion of a catheter.

[0024] The bioabsorbable polymers include polylactic acid (PLA), polyglycol acid (PGA), polyglactin (polyglycol acid - polylactic acid copolymer), polydioxanone, polyglyconate (trimethylene carbonate - glycolide copolymer), and a copolymer of ϵ -caprolactone with polyglycol acid or polylactic acid.

[0025] A variety of materials, including pharmaceuticals, may be mixed into the bioabsorbable polymer. These materials may also be affixed to the fiber surface.

[0026] The luminal stent of the present invention is inserted into the site of vasculogenesis via a catheter fitted with a balloon and is mounted in place by being extended as a result of inflation of the balloon. Although the shape of the luminal stent thus inserted is maintained for several weeks to several months after the insertion, it is formed of the bioabsorbable polymer fibers and hence disappears by being absorbed into the living tissue after the lapse of several months after the insertion.

[0027] In addition, if a material impermeable to X-rays is mixed into the bioabsorbable polymer, the state of the luminal stent may be recognized on irradiation of X-rays from outside after its insertion.

[0028] The luminal stent of the present invention essentially consists of a single yarn entwined around the peripheral surface of a tubular member into a tubular form without weaving or knitting the yarn. Although the yarn is entwined around the peripheral surface of the tubular member, it is not in the wound or coiled state around the tubular member. That is, the yarn of the bioabsorbable polymer fibers is meandered as shown in Fig. 1a or coiled into one or more loops, as shown in Figs. 1b to 1g, for forming a planar yarn mass formed by meandered and/or coiled bioabsorbable polymer fibers, which yarn mass is entwined around the tubular

member for producing a fiber mass extending along a curved surface.

[0029] Fig.2 shows an example of a luminal stent according to the present invention in which a meandering yarn formed of bioabsorbable polymer fibers is shaped into a tube. Fig.3 shows another example of a luminal stent according to the present invention in which a meandering yarn formed of bioabsorbable polymer fibers is similarly shaped into a tube.

[0030] When transporting the luminal stent of the present invention to a target site, it can be passed through various meandering vessels substantially more easily than the metal stent or the woven or knitted textile stent. That is, the luminal stent prepared from the yarn formed of bioabsorbable polymer fibers is able to follow any meandering path with excellent trackability, while it can be inserted as far as and fixed at a bent site because the yarn formed into a tubular shape by meandering without being woven or knitted exhibits strong extensibility and is not likely to injure the cavity. According to the present invention, in order for the luminal stent in the shape of a tube about 5 mm in diameter to be introduced into a vessel of the living body which is lesser in diameter, the tube is heat-set by heat treatment and thereby shrunk to a diameter of approximately 2 mm or less. The process is illustrated in Fig.4.

[0031] The heat-set luminal stent is inserted into the vessel in the manner shown in Fig.5, as will be explained subsequently,

[0032] Fig.6 shows another method of contracting the diameter of a luminal stent formed by shaping the yarn of PGA (polyglycol acid) polymer fibers. The method shown in Fig.6 has an advantage in that, since a tube formed of a heat-resistant resin or metal is not employed, the stent may be directly introduced into and fixed at a balloon forming area in the vicinity of a foremost part of a catheter.

[0033] The tubular luminal stent prepared by shaping a yarn of bioabsorbable polymer fibers has a diameter of approximately 4 to 5 mm and is heat-set by being housed in or gradually introduced into a tube of a heat-resistant resin or metal having an inner diameter of 1 to 3 mm and preferably 2 mm for producing a luminal stent having a diameter of approximately 2 mm, as shown in Fig.4.

[0034] In addition, the tubular luminal stent may be heat-set while in the larger diameter. Alternatively, the tubular luminal stent may be reduced in diameter and heat-set for maintaining good shaping properties. The heat setting not only is effective for maintaining the shape of the luminal stent but is meaningful in minimizing the stress applied to the inner wall of the vessel of the living body.

[0035] Meanwhile, by forming the bioabsorbable polymer fibers of PLA and PGA, and changing their mixing ratio, the time period required for the strength of the luminal stent of the present invention to be decreased to one-half of the original strength, or the time period until

extinction of the luminal stent through absorption into the living body, may be freely controlled within a range from three weeks to three months.

[0036] If an agent impermeable to X-rays is mixed into the fibers at the time of spinning the fibers into a yarn, the state of insertion of the luminal stent can be observed by the X-rays. Thrombolytic agents or anti-thrombotic agents, such as heparin, urokinase or t-PA, may also be mixed for optimum effects.

[0037] Furthermore, since the luminal stent of the present invention is formed of the yarn of bioabsorbable polymer fibers, and hence it disappears from the site of vasculogenesis in a preset period, carcinostatic agents or various other pharmaceutical may be mixed into or affixed on the fibers for concentrated administration of the pharmaceutical to the site of lesion.

[0038] In addition, the fibers making up the luminal stent of the present invention may be variegated in the cross-sectional shape thereof more easily than in the case of preparing the luminal stent of metal. That is, by setting the cross-sectional shape of the filaments on spinning so as to be of a hollow or profiled shape, such as an elliptical or a flower petal shape, or by employing singular or multiple monofilaments, it becomes possible to control bio-compatibility or shape retention characteristics.

[0039] The yarn formed of a synthetic high molecular material may have its fiber surface processed in desired manner. With the yarn having the usual substantially circular cross-section and having its surface not processed in any particular manner, the yarn having the so-called profiled cross-section, or the yarn processed as described above, it becomes possible to deposit an anti-thrombotic material or a thrombolytic agent on the yarn or cells of the living body to promote multiplication of the endothelial cells of the living body or to a material impermeable to X-rays. In this case, longitudinally extending flutes or a variety of recesses may be formed on the yarn surface for improving the deposition efficiency.

[0040] If it is desired to increase the diameter of a constricted portion of the vessel to a diameter of, for example, 4 mm and to maintain this diameter, it is not increased at a time. That is, for avoiding the sudden stress being applied to the vessel and to the living body, the vessel is expanded initially to a diameter of 3 mm, using an expander having a balloon-forming portion having a diameter of approximately 0.8 to 1.2 mm, after which the catheter provided with a balloon is extracted. A catheter provided with a balloon, which catheter is not fitted with a luminal stent and is capable of only forming a balloon, is again inserted for enlarging the vessel to a diameter slightly larger than 4 mm. Subsequently, a luminal stent is introduced and fixed at the balloon forming portion using a device for inserting and fixing the luminal stent of the present invention.

[0041] It is unnecessary to expand and form the vessel stepwise. Thus, it is possible to expand the constricted portion of the vessel at a time to a desired diameter

and subsequently proceed to the fitting of the luminal stent.

[0042] On the other hand, the luminal stent fitting device itself, consisting in a catheter fitted with a balloon and a luminal stent of the present invention fitted thereon, may be used for inserting and fixing the luminal stent in the vessel of the living body simultaneously with expansion of the vessel.

[0043] The device for inserting and fixing the luminal stent of the present invention in a constricted portion of the vessel of the living body is explained in detail. There is an area 3 in the vicinity of the distal end of a catheter 2 in which a balloon of a desired diameter may be formed by the liquid or the gas, such as an X-ray contrast medium, which is injected from a hollow portion in the catheter at a liquid pressure of 8 to 10 atmospheres, as shown in Fig.5. It is over this balloon-forming area 3, which is about 20 mm long, that a luminal stent 11 about 2 mm in diameter, as heat-set, is applied.

[0044] It is noted that the length of the balloon-forming area 3 or the diameter of the luminal stent 11 may be optionally set depending on the type of the vessel to be treated or the specific properties of the vessel.

[0045] Meanwhile, a guide wire acting as a leading wire when inserting the catheter into the vessel of a living body is occasionally mounted on the distal end of the catheter.

[0046] As for the insertion of the luminal stent, a mid part along the length of the balloon-forming area of the catheter is formed with a communication orifice via which the fluid injected for balloon formation is caused to flow out at the mid portion of the catheter so as to be charged into a space between it and a thin film forming the balloon. It is via this orifice that the balloon is formed under a fluid pressure of 8 to 10 atmospheres, with the ballooned state being kept for 30 to 60 seconds and occasionally for a longer time duration. At this time, the balloon undergoes a kind of plastic deformation and is maintained under the inflated condition under the inflating pressure exerted by the balloon. The inflated shape is maintained by changes in the polymer itself on the molecular level or the yarn shaped into a tube is expanded in the radial direction for maintaining the expanded shape.

[0047] Fig.5 shows the process of inserting and fitting the luminal stent of the present invention in the vessel of a living body. As shown therein, the balloon is inflated and subsequently contracted to permit the catheter 2 in its entirety to be withdrawn from the luminal stent.

[0048] Fig. 7 shows another embodiment of a luminal stent inserting and fitting device according to the present invention. A catheter fitted with a balloon, on which the luminal stent 11 is subsequently wrapped, is encased within a sheath 5. The resulting assembly is inserted into the vessel of the living body. The sheath is extracted slightly and the balloon is inflated and maintained in the inflated state. The balloon is contracted and the sheath 5 is extracted along with the catheter 2 so that the lumi-

nal stent is left in the vessel of the living body.

[0049] Meanwhile, the film for balloon formation may be formed of any of a variety of synthetic high molecular material, such as polyethylene terephthalate or polyethylene.

[0050] It is noted that the luminal stent of the present invention may be inserted and fitted in a bend of the vessel to conform to its shape, as shown in Fig.8. The state of the stent as inserted and fitted is shown in Fig.8B. A metal stent formed of a woven or knitted textile of linear longitudinal and transverse materials and subsequently formed into a tubular form is shown in Fig. 8C in the state of being inserted into and fitted in a bend of the vessel. Such stent is flexed in the bend of the vessel so that the normal shape of the vessel cannot be maintained at the site. Conversely, the luminal stent of the present invention is able to follow a branched section in the vessel with good trackability so that it can reach any constricted site in the vessel, as discussed previously.

[0051] In Fig.8A, showing a typical shape of the vessel of a living body, the site shown by an arrow a represents a site assumed to be the mounting site for the luminal stent of the present invention.

[0052] The luminal stent of the present invention, as formed by the yarn of the bioabsorbable polymer fibers and heat-set, may be adapted to a vessel of an arbitrary thickness by means of the luminal stent inserting and fixing device according to the present invention. If it is assumed that the luminal stent is applied to a site where the vessel is enlarged to a diameter of approximately 4 mm or larger on inflation of the balloon, the luminal stent may be applied to the vessel site having the diameter of 2.5 mm by controlling the degree of inflation of the balloon. The luminal stent may similarly be applied to a vessel site having the diameter of 3 to 4 mm. That is, the luminal stent may be applied to any site shown in Fig.9 using the same catheter provided with the balloon. The reason is that the inner diameter of the luminal stent may be maintained at a diameter corresponding to the diameter of the inflated balloon.

[0053] If vessel re-constriction is produced in several months after the luminal stent of the present invention is decomposed and absorbed to the living body, the luminal stent may be applied again to the same site because the stent is formed of biodegradable and absorbable polymer material.

[0054] The luminal stent of the present invention, as described above, is not susceptible to inflammation or excess hypertrophy of the vessel, and hence the re-constriction may be prevented from occurrence. In addition, the luminal stent is compatible with the living body because it is vanished in several months by being absorbed by the living tissue.

[0055] If an agent impermeable to X-rays is applied to the bioabsorbable polymer fibers or the yarn, the state of insertion of the luminal stent may be checked easily by irradiation of X-rays from outside.

[0056] Also, the luminal stent may be applied on the

balloon-forming portion of the catheter provided with th balloon according to the present invention for inserting and fitting the stent at any desired location in the vessel.

[0057] Meanwhile, if the luminal stent of the present invention is applied over the balloon-forming portion of the catheter fitted with the balloon for fixing the stent at a desired site in the vessel, it may occur that the fixing position of the luminal stent is deviated due to contact of the stent with the inner wall of the vessel. If the luminal stent is deviated in its position and disengaged from the balloon forming region, it becomes difficult to realize an optimum expanded position.

[0058] Thus it is desirable to apply a bio-compatible material on the luminal stent applied over the balloon-forming region by way of "sizing" for immobilizing the luminal stent at the balloon forming region. The material that may be employed as an adhesive or sizing agent is a bio-compatible material enumerated by an *in vivo* decomposable polymer, such as polylactic acid (PLA), water-soluble protein, such as gelatin, or fibrin sizing agent.

[0059] If, for example, PLA is dissolved as a solute in a solvent to give a solution which is coated on the stent and dried, the solution is left as a solid film to play the role of an adhesive. However, this method cannot be applied to the PLA stent because the PLA stent is dissolved in the solution. Thus it is necessary to employ some other bio-compatible material for the PLA stent.

[0060] Meanwhile, the bio-compatible material, used as the adhesive, may be applied to the stent in its entirety, or only to the overlapped region of the bioabsorbable polymer fibers.

Experiment 1

[0061] A yarn of polylactic acid fibers, admixed with barium sulfate, was meandered and applied to the peripheral surface of a tubular-shaped member to form a luminal stent. A plurality of such luminal stents, each being 4 mm in diameter and 20 mm in length, were applied to the coronary artery of a test animal, using a catheter fitted with a balloon. Observation by X-ray radiation revealed that the shape of the stent was maintained substantially unchanged for about 3 to 6 months and disappeared in about 6 to 12 months by being absorbed by the living tissue. During this period, inflammation or excess hypertrophy of the endothelial cells of the blood vessel was not observed.

Experiment 2

[0062] A yarn of polyglycol acid fibers, admixed with barium sulfate, was looped to be a plane-shaped and applied to the peripheral surface of a tubular-shaped member to form a luminal stent. A plurality of such luminal stents, each being 4 mm in diameter and 20 mm in length, were applied to the femoral artery of a test animal. Observation by X-ray radiation revealed that th

shape of the stent was maintained substantially unchanged for about 2 to 6 weeks and absorbed by the living body in about 2 to 3 months. During this period, inflammation or excess hypertrophy of the endothelial cells of the blood vessel was not observed.

Claims

1. A luminal stent in which a continuous bioabsorbable polymer material is formed in a non-woven non-knitted meandering state in a shape conforming to peripheral surface of an imaginary tubular member, **characterized in that** said polymer material is formed of a yarn of continuous bioabsorbable polymer fibers.
2. The luminal stent as claimed in claim 1, **characterized in that** the bioabsorbable polymer is at least one selected from the group consisting of polylactic acid, polyglycol acid, polyglactin (polyglycol acid - polylactic acid copolymer), polydioxanone, polyglyconate (trimethylene carbonate - glycolide copolymer), and a copolymer of ϵ -caprolactone with polyglycol acid or polylactic acid.
3. The luminal stent as claimed in claim 1 or 2, **characterized in that** the bioabsorbable polymer fibers are circular, non-circular or hollow in cross-section.
4. The luminal stent as claimed in anyone of claims 1 to 3, **characterized in that** the bioabsorbable polymer fibers present surface irregularities.
5. The luminal stent as claimed in anyone of claims 1 to 4, **characterized in that** at least one of an agent impermeable to X-rays, a carcinostatic agent and an anti-thrombotic agent is mixed into the bioabsorbable polymer fibers.
6. The luminal stent as claimed in anyone of claims 1 to 5, **characterized in that** at least one of an agent impermeable to X-rays, a carcinostatic agent, an anti-thrombotic agent and cells of a living body is deposited on the surface of the bioabsorbable polymer fibers.
7. A method for producing a luminal stent as claimed in anyone of claims 1 to 6, comprising:

guiding a planar mass formed of a yarn of bioabsorbable polymer fibers along the peripheral surface of a tubular member for shaping said planar mass substantially into a tubular member presenting a curved surface.
8. The method for producing the luminal stent as claimed in claim 7, further comprising heat-setting

the tubular member having the curved surface for reducing the diameter of the tubular member as compared to the diameter during shaping.

- 5 9. A combination of a luminal stent as claimed in any one of claims 1 to 6 and a device for applying a luminal stent comprising a catheter having a balloon-forming portion (3) at a distal end thereof and the luminal stent (11) said luminal stent being fitted over said balloon-forming portion (3).
- 10 10. The combination as claimed in claim 9, wherein the luminal stent (11) is coated with a bio-compatible material and thereby affixed to the balloon-forming portion (3).
- 15 11. The combination as claimed in claim 10, **characterized in that** the bio-compatible material is at least one selected from an in vivo decomposable polymer, a water-soluble polymer, water-soluble protein and fibrin sizing agent.
- 20 12. The combination as claimed in claim 10, **characterized in that** the bio-compatible material is polylactic acid (PLA).
- 25

Patentansprüche

- 30 1. Gefäßstent, bei dem ein kontinuierliches, biologisch absorbierbares Polymermaterial in schlangelinienförmigem, nicht gewirkten Vlieszustand zu einer Form geformt ist, die zur Umfangsfläche eines gedachten rohrförmigen Elements passt, **dadurch gekennzeichnet, dass** das Polymermaterial aus einem Garn aus kontinuierlichen, biologisch absorbierbaren Polymerfasern besteht.
- 35 2. Gefäßstent nach Anspruch 1, **dadurch gekennzeichnet, dass** das biologisch absorbierbare Polymer mindestens eines ist, das aus der aus Folgendem bestehenden Gruppe ausgewählt ist: Polymilchsäure, Polyglycolsäure, Polyglactin (Polyglycolsäure-Polymilchsäure-Copolymer), Polydioxanon, Polyglyconat (Trimethylencarbonat-Glycolid-Copolymer) und einem Copolymer von ϵ -Caprolacton mit Polyglycolsäure oder Polymilchsäure.
- 40 3. Gefäßstent nach Anspruch 1 oder 2, **dadurch gekennzeichnet, dass** die biologisch absorbierbaren Polymerfasern kreisförmigen, nicht kreisförmigen oder hohlen Querschnitt aufweisen.
- 45 4. Gefäßstent nach einem der Ansprüche 1 bis 3, **dadurch gekennzeichnet, dass** die biologisch absorbierbaren Polymerfasern Unregelmäßigkeiten an der Oberfläche aufweisen.
- 50
- 55

5. Gefäßstent nach einem der Ansprüche 1 bis 4, **dadurch gekennzeichnet, dass** ein für Röntgenstrahlung undurchlässiges Mittel, ein krebshemmendes Mittel und/oder ein Antithrombosemittel in die biologisch absorbierbaren Polymerfasern eingemischt ist.
6. Gefäßstent nach einem der Ansprüche 1 bis 5, **dadurch gekennzeichnet, dass** ein für Röntgenstrahlung undurchlässiges Mittel, ein krebshemmendes Mittel, ein Antithrombosemittel und/oder Zellen eines lebenden Körpers auf der Oberfläche der biologisch absorbierbaren Polymerfasern abgedeckt sind.
7. Verfahren zum Herstellen eines Gefäßstents, wie er in einem der Ansprüche 1 bis 6 beansprucht ist, umfassend:
 - Führen einer planaren Masse aus einem Garn biologisch absorbierbarer Polymerfasern entlang der Umfangsfläche eines rohrförmigen Elements zum Formen der planaren Masse zu im Wesentlichen einem rohrförmigen Element, das eine gekrümmte Fläche aufweist.
8. Verfahren zum Herstellen eines Gefäßstents nach Anspruch 7, ferner umfassend ein Verfestigen des rohrförmigen Elements mit der gekrümmten Fläche durch Wärme, um den Durchmesser desselben im Vergleich zum Durchmesser während des Formens zu verringern.
9. Kombination aus einem Gefäßstent nach einem der Ansprüche 1 bis 6 mit einer Vorrichtung zum Applizieren eines Gefäßstents, mit einem Katheter mit einem Ballonerzeugungsabschnitt (3) an seinem distalen Ende und dem Gefäßstent (11), der auf den Ballonerzeugungsabschnitt (3) aufgebracht ist.
10. Kombination nach Anspruch 9, bei der der Gefäßstent (11) mit einem biologisch verträglichen Material beschichtet und dadurch am Ballonerzeugungsabschnitt (3) befestigt ist.
11. Kombination nach Anspruch 10, **dadurch gekennzeichnet, dass** das biologisch verträgliche Material mindestens eines ist, das aus Folgendem ausgewählt ist: einem in vivo zersetzbaren Polymer, einem wasserlöslichen Polymer, einem wasserlöslichen Protein und einem Fibrinleim.
12. Kombination nach Anspruch 10, **dadurch gekennzeichnet, dass** das biologisch verträgliche Material Polymilchsäure (PLA) ist.

R revendications

1. Dilatateur de lumière pour lequel on donne à un matière polymère bioabsorbable continue une forme sinueuse, non tissée et non tricotée, correspondant à la surface périphérique d'un élément tubulaire imaginaire, **caractérisé en ce que** la matière polymère se compose d'un fil de fibres polymères bioabsorbables continues.
2. Dilatateur de lumière selon la revendication 1, **caractérisé en ce que** le polymère bioabsorbable est au moins l'un des éléments choisis dans le groupe constitué de poly(acide lactique), poly(acide glycolique), polyglactine [copolymère poly(acide glycolique-poly(acide lactique))], polydioxanone, polyglyconate (copolymère de triméthylène carbonate-glycolide) et copolymère de l'é-caprolactone avec le poly(acide glycolique) ou le poly(acide lactique).
3. Dilatateur de lumière selon la revendication 1 ou 2, **caractérisé en ce que** les fibres polymères bioabsorbables ont une section transversale circulaire, non circulaire ou creuse.
4. Dilatateur de lumière selon l'une quelconque des revendications 1 à 3, **caractérisé en ce que** la surface des fibres polymères bioabsorbables présente des aspérités.
5. Dilatateur de lumière selon l'une quelconque des revendications 1 à 4, **caractérisé en ce qu'on** mélange aux fibres polymères bioabsorbables l'un au moins des agents suivants : agent imperméable aux rayons X, agent carcinostatique et agent antithrombose.
6. Dilatateur de lumière selon l'une quelconque des revendications 1 à 5, **caractérisé en ce qu'on** dépose sur la surface des fibres polymères bioabsorbables l'un au moins des éléments suivants : agent imperméable aux rayons X, agent carcinostatique, agent anti-thrombose et cellules d'un corps vivant.
7. Méthode pour produire un dilatateur de lumière selon l'une quelconque des revendications 1 à 6, consistant à :
 - guider une masse plane composée d'un fil de fibres polymères bioabsorbables le long de la surface périphérique d'un élément tubulaire pour donner globalement à ladite masse plane la forme d'un élément tubulaire présentant une surface courbe.
8. Méthode pour produire le dilatateur de lumière selon la revendication 7, prévoyant également l' ther-

mofixage de l'élément tubulaire à surface courbe pour réduire son diamètre par rapport au diamètre qu'il présente pendant son formage.

9. Combinaison d'un dilateur de lumière selon l'une 5
quelconque des revendications 1 à 6 et d'un dispo-
sitif pour appliquer un dilateur, comprenant un ca-
théter pourvu à son extrémité distale d'une partie
formant ballon (3) et ledit dilateur (11), ce dernier
étant installé sur la partie formant ballon (3). 10
10. Combinaison selon la revendication 9, dans laquel- 15
le le dilateur (11) est revêtu d'une matière biocom-
patible et est ainsi fixé à la partie formant ballon (3).
11. Combinaison selon la revendication 10, **caractéri-
sée en ce que** la matière biocompatible est au
moins une matière choisie parmi un polymère dé-
composable in vivo, un polymère soluble dans
l'eau, une protéine soluble dans l'eau et un agent 20
adhésif à base de fibrine.
12. Combinaison selon la revendication 10, **caractéri-
sée en ce que** la matière biocompatible est consti-
tuée par le poly(acide lactique) (PLA). 25

30

35

40

45

50

55

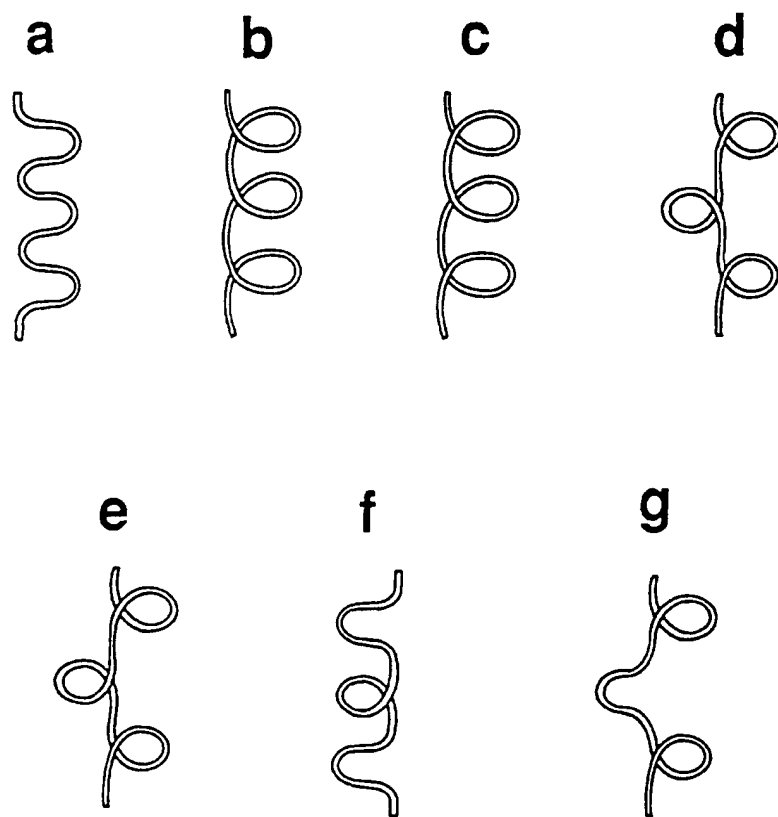


FIG.1

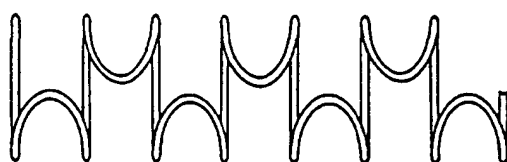


FIG.2

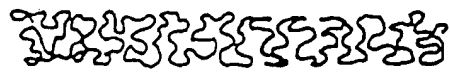


FIG.3

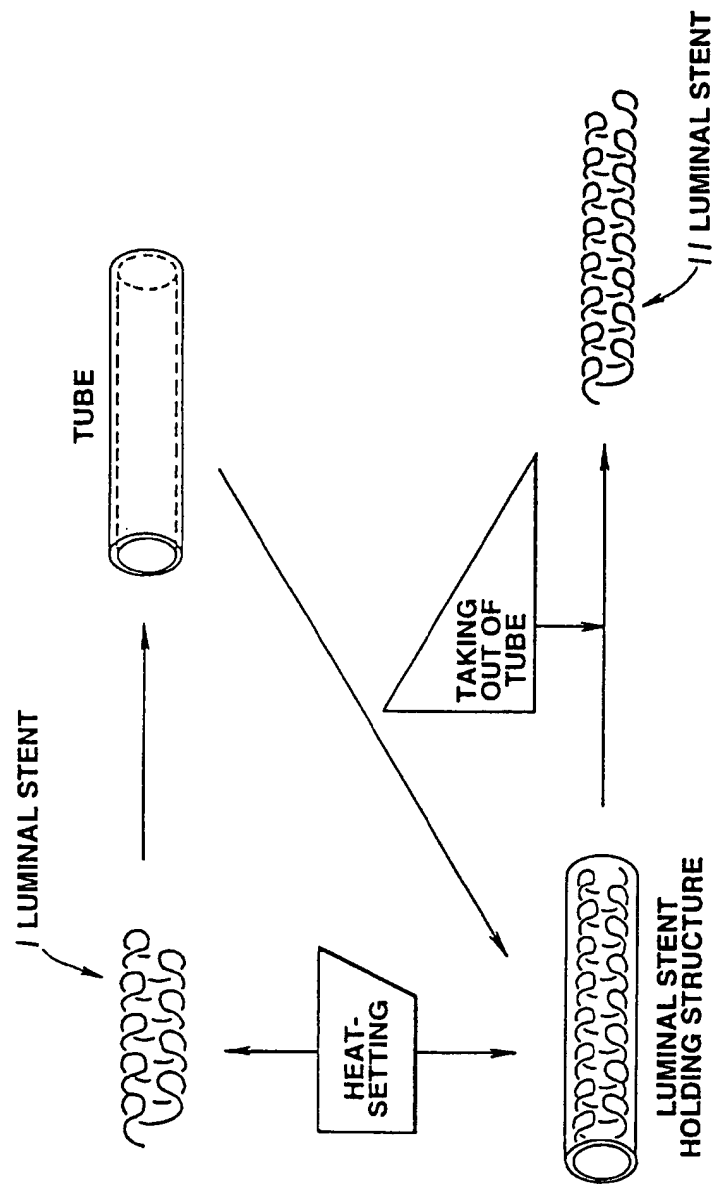


FIG.4

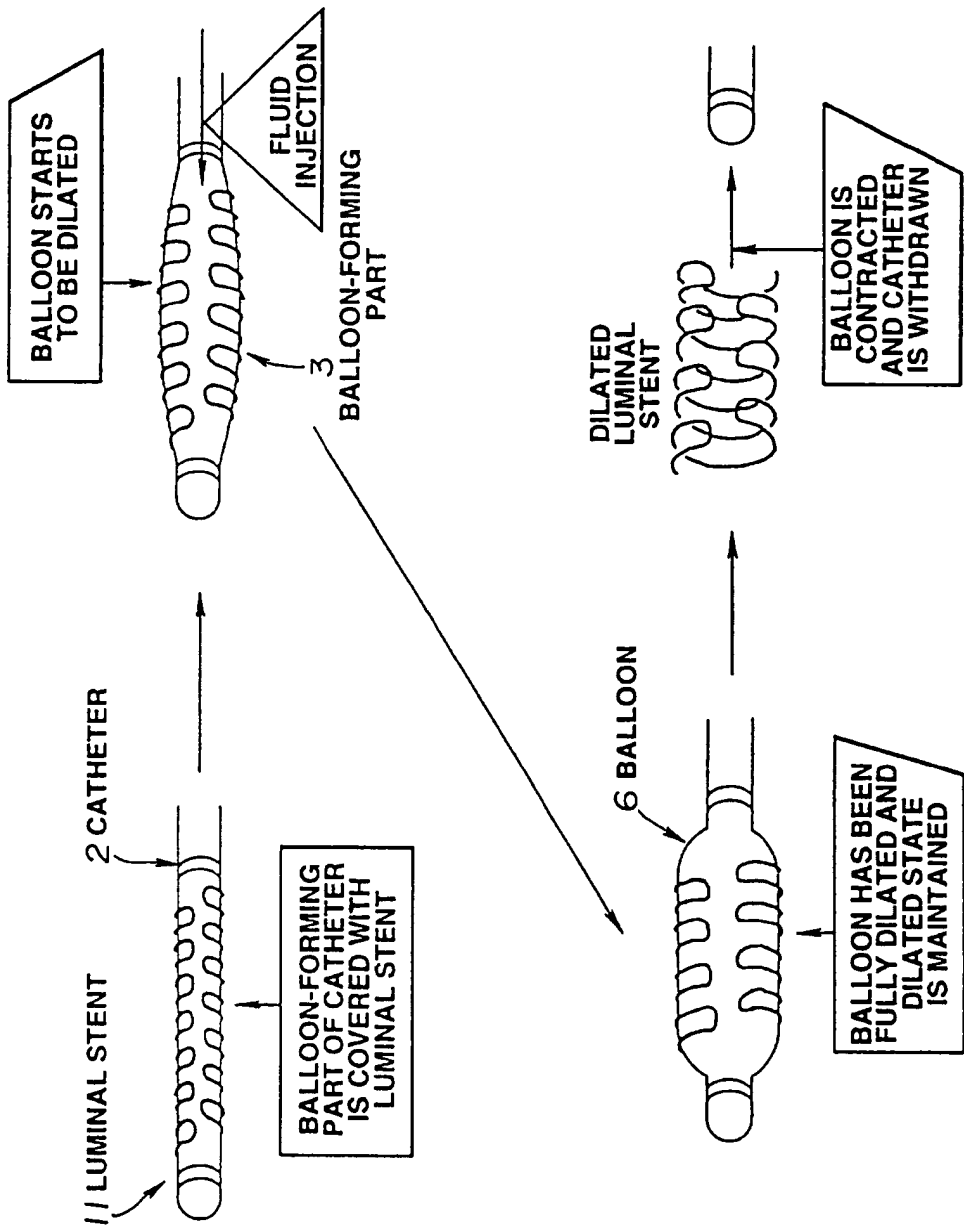


FIG.5

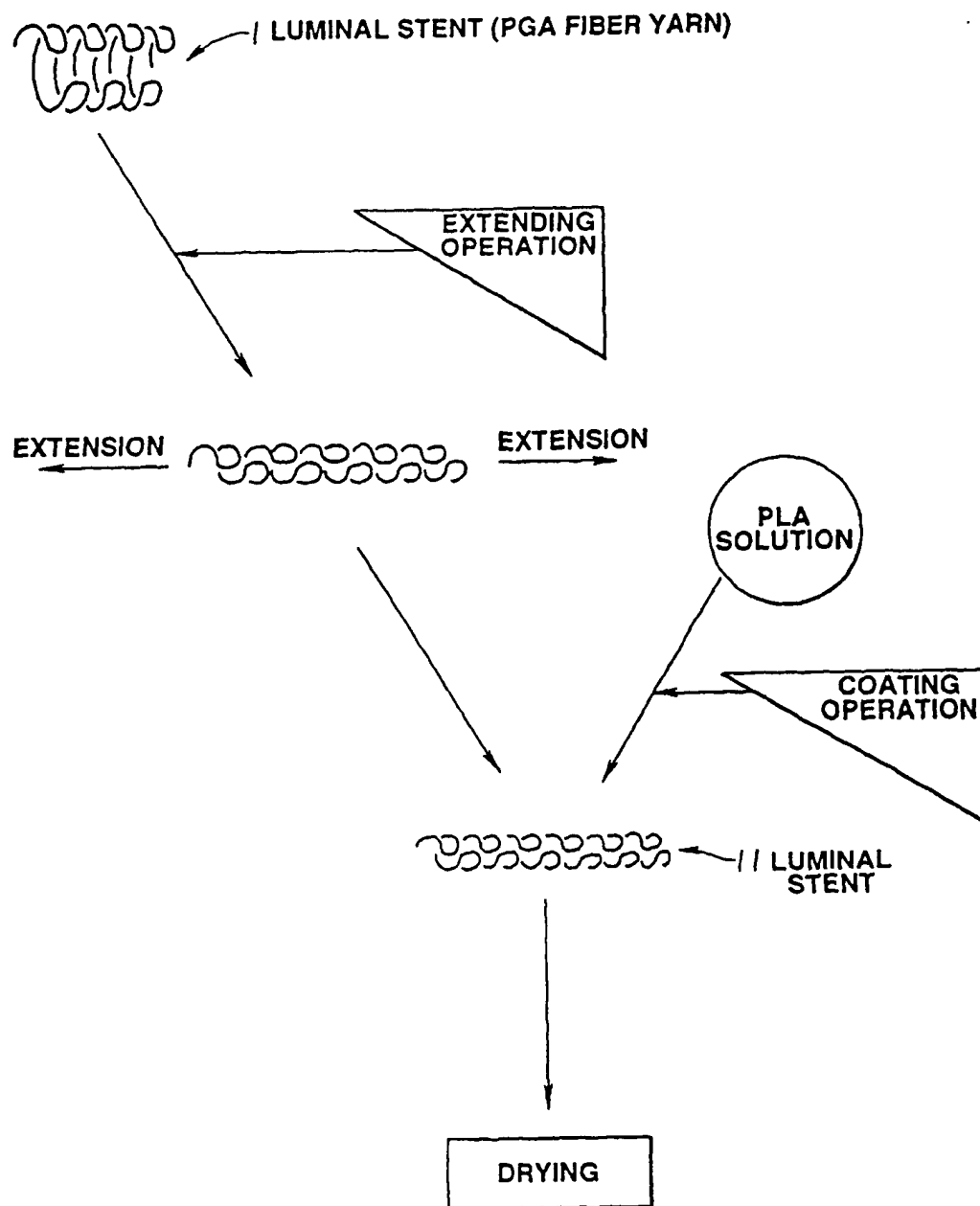


FIG.6

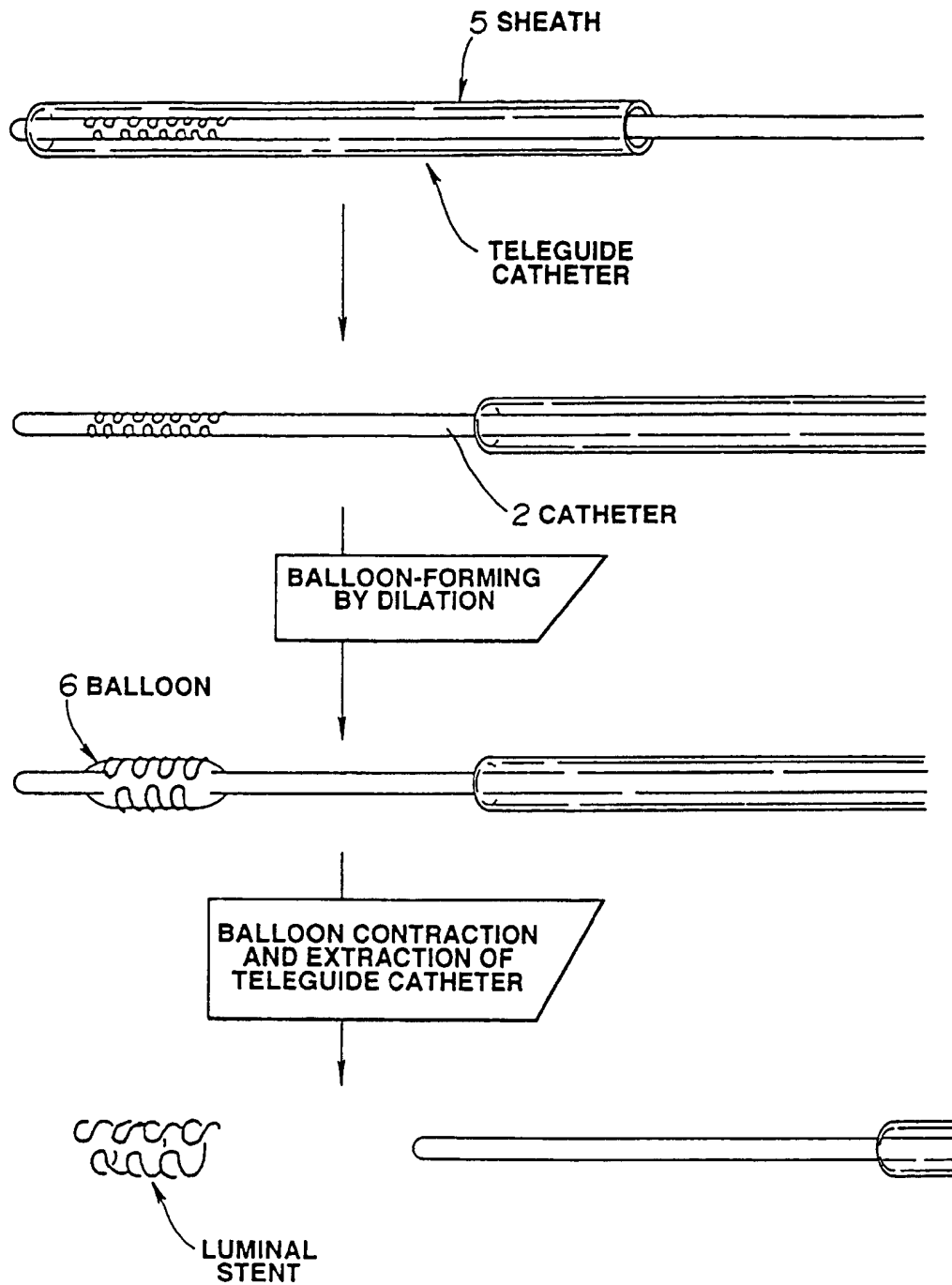


FIG.7

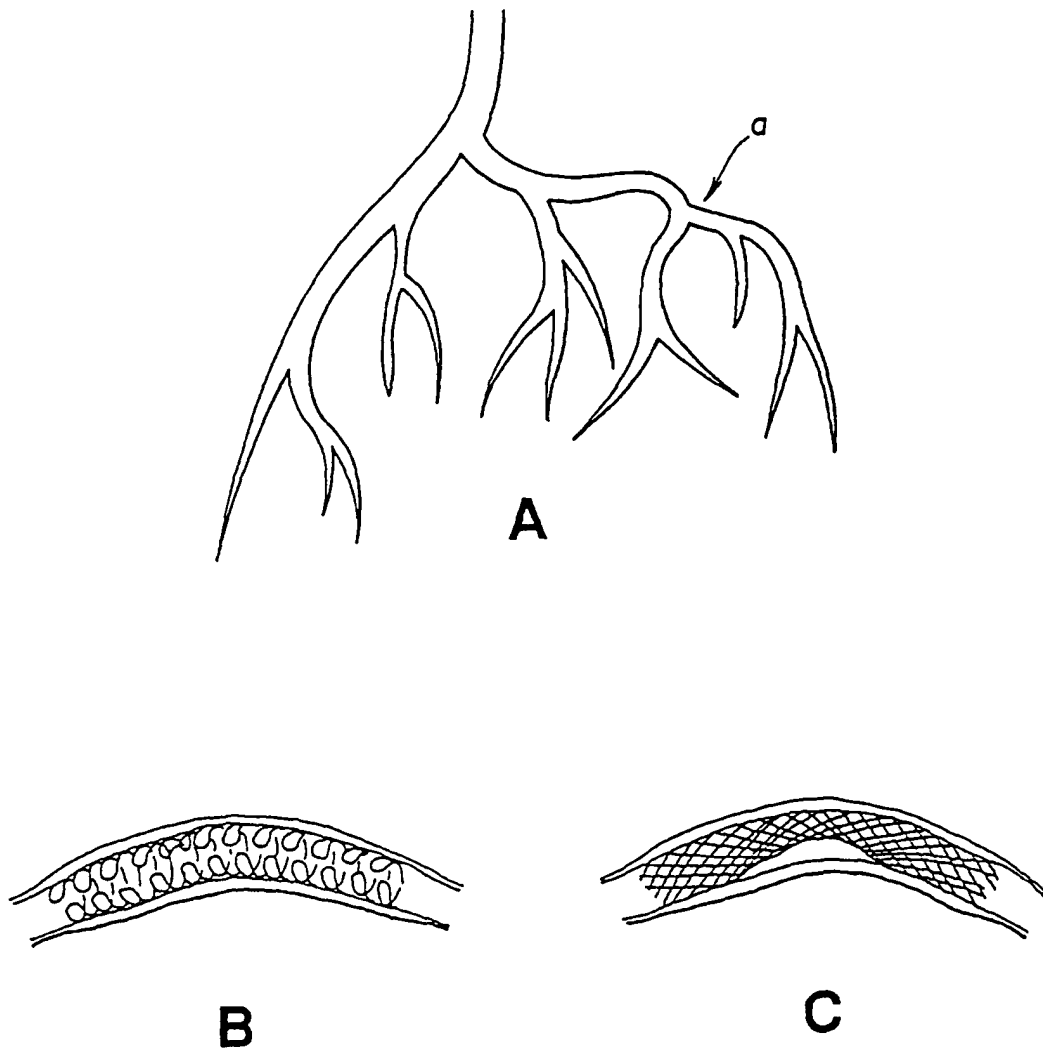


FIG.8

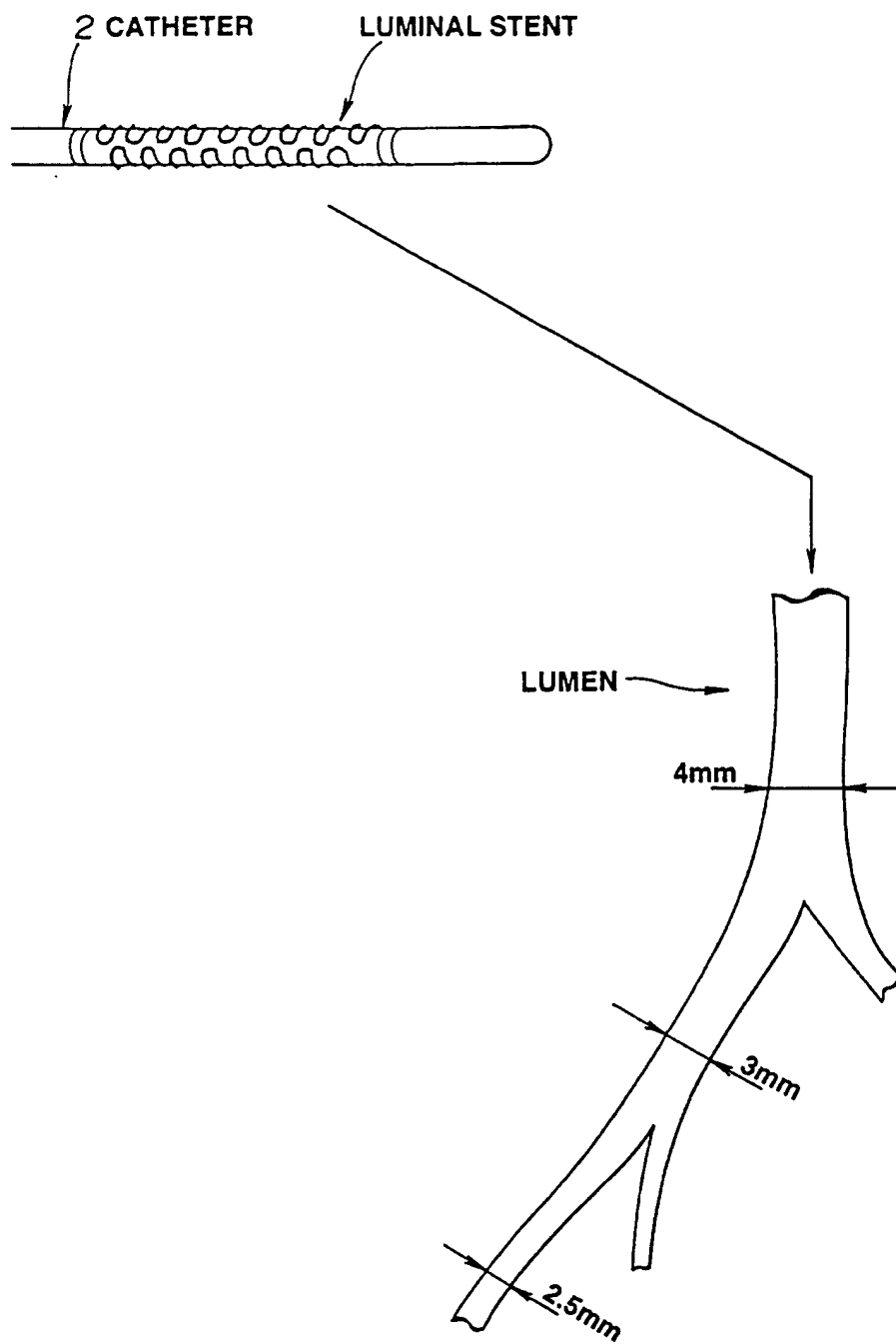


FIG.9